

## Original Research

### A novel label-free cocaine assay based on aptamer-wrapped single-walled carbon nanotubes

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#### Abstract

**Objective(s):** This paper describes a selective and sensitive biosensor based on the dissolution and aggregation of aptamer wrapped single-walled carbon nanotubes. We report on the direct detection of aptamer–cocaine interactions, namely between a DNA aptamer and cocaine molecules based on near-infrared absorption at  $\lambda_{807}$ .

**Materials and Methods:** First a DNA aptamer recognizing cocaine was non-covalently immobilized on the surface of single walled carbon nanotubes and consequently dissolution of SWNTs was occurred. Vis-NIR absorption ( $A_{807nm}$ ) of dispersed, soluble aptamer-SWNTs hybrid, before and after incubation with cocaine was measured using a CECIL9000 spectrophotometer.

**Results:** This carbon nanotube setup enabled the reliable monitoring of the interaction of cocaine with its cognate aptamer by aggregation of SWNTs in the presence of cocaine.

**Discussion:** This assay system provides a mean for the label-free, concentration-dependent, and selective detection of cocaine with an observed detection limit of 49.5 nM.

**Keywords:** Aptamer, Cocaine, Near infrared absorption, Single-walled carbon nanotube

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### Introduction

Simple and sensitive detection of cocaine is very important to fight against the illegal usage of this compound. However, this has remained as a bottleneck in cocaine identification and quantification until the development of specific aptamers against it (1-9). Nowadays aptamers are of increasing interest in being used as recognition element within sensors for small molecules (10-13). Aptamers exhibit several advantages such as high affinity and specificity with respect to target recognition. Moreover, in comparison with antibodies, they are resistant to cycles of denaturation-renaturation, and are less prone to degradation. Furthermore, they can be chemically synthesized and, thus, adopted to develop biosensors.

So far several nucleic acid aptamer-based biosensors for cocaine detection have been developed. The cocaine quantification approach in developed aptameric biosensor was mainly based on colorimetric (1-4), electrochemical (5) and fluorescence techniques (6-9).

However, these reported aptameric sensors either exhibit relatively hard sample preparation, inadequate sensitivity, or high sample consumption. Consequently, the development of alternative simple and sensitive aptameric sensors is highly desirable.

Single-walled carbon nanotubes (SWNT) exhibit excellent optical properties, including Raman light scattering, near-infrared (NIR) fluorescence and NIR absorption (14-16).

The optical properties of SWNT make them suitable to be employed for the development of biological sensors due to their NIR photoluminescence/absorption where absorption and auto-fluorescence by tissues, biological fluids and water are minimized (17, 18). Although SWNTs have near-infrared (NIR) absorption and photoluminescence properties which make them interesting as biosensor but their

photoluminescence is observed only when they are individually dispersed (19).

CNTs are extremely hydrophobic and are insoluble in water.

Two methods have been employed to modify the hydrophobic surface of CNTs to increase their solubility.

The first was to disperse carbon nanotubes in aqueous solution by covalent association of water soluble materials to the CNT surface, and the second approach was used the noncovalent association of materials to the CNT surface (20-26).

In both approaches, various organic or biological materials have been utilized successfully including oligonucleotides (27), peptides (28) and proteins (29).

Meanwhile, covalent association of materials to the surface of CNTs is appropriate for many applications, although one important disadvantage is that the covalent association introduces defects in the surface of the CNTs that often interfere with the electronic and optical properties. Thus non-covalent attachment of materials to CNTs is more appropriate for increasing their solubility.

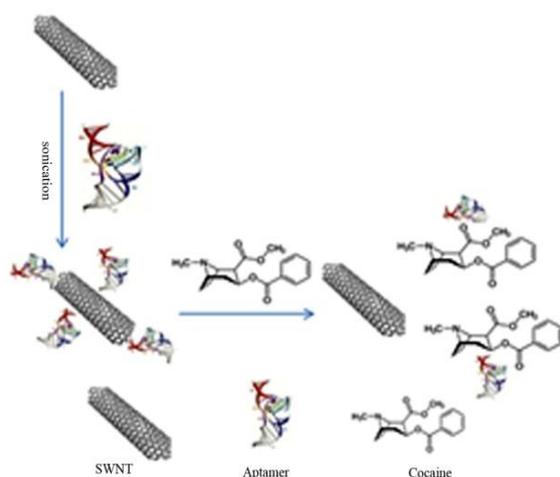
In the case of aptamer-wrapped carbon nanotubes, the structural change in nucleic acid aptamers upon interaction with target molecules sufficiently perturbs the electronic structure of SWNTs such that the change can be detected optically (30).

In current study, aptamers were immobilized non-covalently on the surface of SWNTs via  $\pi$ -stacking interactions between the nucleotide bases and the SWNT sidewalls and the specific interaction of aptamers wrapped on the sidewall of SWNTs with cocaine was detected via near-infrared absorption (Figure 1).

### Materials and Methods

#### General

All chemicals and reagents were purchased from Sigma Aldrich (Germany) with the highest quality available.



**Figure 1.** Schematic illustration of aptameric sensor for cocaine sensing. Cocaine aptamer was noncovalently attached to SWNTs. Upon cocaine interaction, aptamer was unwrapped from SWNTs and the changes in carbon nanotubes solubility were detected.

### **Synthesis of aptamer**

An anti cocaine ssDNA aptamer (5' GACAAGGAAAATCCTTCAATGAAGTGGGTC 3') reported by Cekan and colleagues (31) was employed as bioreceptor.

Cocaine ssDNA aptamer was synthesized using standard phosphoramidate chemistry and purified by polyacrylamide denaturing gel electrophoresis to remove the truncated DNA fragments produced in the chemical synthesis.

### **Noncovalent conjugation of aptamer on the surface of SWNTs**

At first stage, SWNTs (0.5 mg) and DNA aptamer (133  $\mu$ M) in 2 ml of Tris-HCl buffer (10 mM, pH 7.4) was sonicated for 2 h. Then mixture was centrifuged at 15000 g for 2 h and pellets containing impurities, aggregates, and bundles of nanotubes were discarded.

Then the supernatant was collected and underwent an additional centrifugation round and finally supernatant containing aptamer-SWNT complexes was collected (32).

### **Quantitative determination of cocaine**

Different concentrations of cocaine (0, 50, 100, 150 and 200 nM) was added to aptamer-SWNT complexes and incubated for 24 h at 37°C.

Vis-NIR absorption ( $A_{807\text{nm}}$ ) of dispersed, soluble aptamer-SWNTs hybrid, before and after incubation with cocaine was measured using a CECIL9000 spectrophotometer (Cecil Company, UK) (32).

## **Results**

### **Purification and characterization of synthesized aptamer**

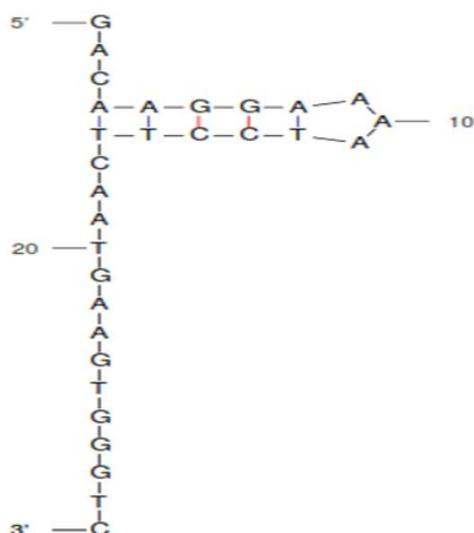
Synthesized DNA aptamer was purified from polyacrylamide denaturing gel (7 M urea) (Figure 2).

$A_{260}/A_{280}$  of synthesized DNA-aptamer and its concentration was 1.83 and 1250 ng/ $\mu$ l, respectively.

Secondary structure of synthesized cocaine aptamer was predicted by Mfold tool (33). As shown in Figure 3, the folded cocaine aptamer contains one hairpin-loop motif and the  $\Delta G$  was - 2.45.



**Figure 2.** Denaturing urea polyacrylamide gel electrophoresis was used to separate and purify synthesized single-stranded DNA aptamer of cocaine. Denaturing PAGE was placed on a fluorescence TLC plate. Aptamers and other truncated oligonucleotides appeared as black bands. Upper band were cut and aptamers were purified by several thaw-freeze cycles.



**Figure 3.** Secondary structure of cocaine ssDNA aptamer as predicted by Mfold ( $\Delta G = -2.45$ ).

### Cocaine determination

Aptamer-SWNT complex was incubated with different concentrations (0-200 nM) of cocaine and the standard curve was plotted at  $\lambda_{807}$  nm.

After adding cocaine into the SWNT–aptamer solution, the UV-Vis-NIR absorption at 807 nm decreased as shown in Figure 4 indicating that the SWNT gradually lost its aptamer-induced dispersion stability and tended to aggregate.

Coefficient of determination ( $r^2$ ) was measured to be 0.987 which demonstrated good linearity between aptamer-SWNTs complex absorption at  $\lambda_{807}$  versus cocaine concentration (Figure 4).

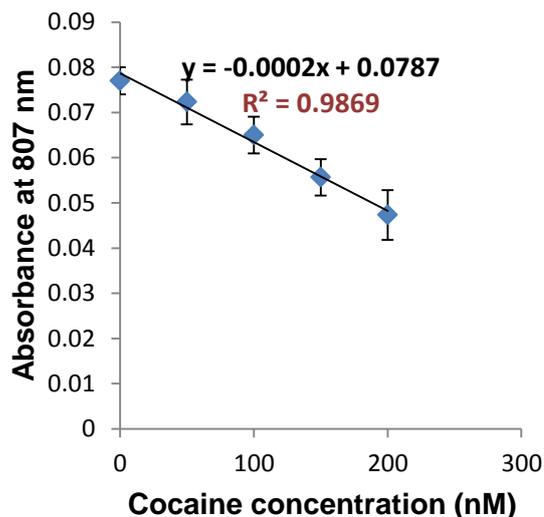
These results clearly indicated that the aggregation fashion was obviously dependent on the concentration of cocaine. The limit of detection (LOD) and limit of quantification (LOQ) was calculated according to equations 1 and 2 where "SD" is standard deviation of the response and "S" is slope of the calibration curve:

$$\text{LOD} = 3.3(\text{SD}/\text{S}) \quad (1)$$

$$\text{LOD}_{(\text{cocaine})} = 3.3(0.003/0.0002) = 49.5 \text{ nM}$$

$$\text{IOQ} = 10(\text{SD}/\text{S}) \quad (2)$$

$$\text{LOQ}_{(\text{cocaine})} = 10(0.003/0.0002) = 150 \text{ nM}$$



**Figure 4.** Standard curve for determination of cocaine using SWNT-based aptameric biosensor.

### Discussion

SWNTs contain extremely delocalized  $\pi$  electrons; consequently the surface of SWNTs can be easily functionalized through  $\pi$ - $\pi$  interactions with compounds that possess a  $\pi$ -electron-rich structure such as nucleic acid aptamers.

Non-covalent association of nucleic acid aptamers to the CNT surface increases its solubility (34).

Previously it was proved that SWNT–aptamer hybrid showed the same semi-conductive band gap between 800 nm to 1350 nm and the electronic properties of SWNT were maintained intact after the DNA wrapping (19).

Furthermore, the solubilized aptamer-wrapped SWNTs are well dispersed, mostly as individual tubes.

After addition of target molecules, aptamers were unwrapped and the amount of soluble SWNTs decreased which could be detected optically.

It is worth mentioning that the main shortcoming using an aptameric sensor for cocaine detection and quantification is its low detection sensitivity which is limited by their relatively low association constant (35).

The best reported detection limits are 10

$\mu\text{M}$ , 5  $\mu\text{M}$  and 0.5  $\mu\text{M}$  of cocaine for various assay techniques including electrochemical method (5), aptamer-based enzymatic assay (6), bulk fluorescence (7) and aptamer-based colorimetric probes (4).

In this regards, Zhou et al. fabricated FITC-labeled aptamer sensor for detection of cocaine. This sensor showed a detection limit of 0.2  $\mu\text{M}$  (36).

The detection limit of our cocaine-aptameric sensor was more desirable than those reported before, with neither complicated sample preparation nor large analyte volume.

It should be noted that most laboratory utilized mass spectral analysis to detect cocaine, which requires the use of stable isotopes as internal standards, very time consuming sample preparation and application of expensive instruments (37, 38).

In contrast, our non-labeled aptameric sensor took advantage of a simple sample preparation, with potential to be applied for simple and low cost detection of cocaine.

## Conclusion

A novel optical cocaine sensor was designed using the reversible dissolution and aggregation of SWNTs based on interaction of cocaine with its specific ssDNA aptamer. Our results revealed that the aptameric sensor was comparatively sensitive with a low detection limit.

Prepared cocaine aptameric sensor works based on optically detection of solubility reduction of aptamer-SWNT hybrids upon binding of aptamer to cocaine.

Thus, developed assay technique did not require either chemical functionalization or labeling of SWNTs and DNA owing to the exclusive NIR absorption at 807 nm of dispersed SWNTs.

With the advances in the development of varieties of aptamers for small molecules, this aptamer-wrapped single-walled carbon nanotube sensor might find wide

application in forensic analysis and clinical diagnostics.

## Acknowledgments

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